

Modeling an angiogenesis treatment after a myocardial infarction - using the discontinuous Galerkin method -

Linda Crapts
September 27, 2012

Outline

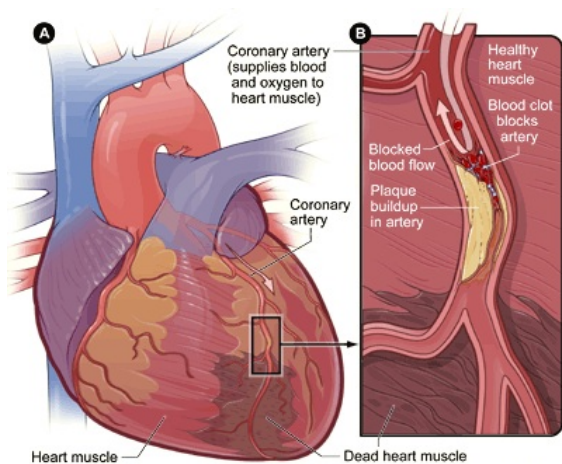
- 1 Biological background
- 2 Mathematical model
- 3 Analytical solutions
- 4 Numerical methods
- 5 Simulations
 - Circular wound
 - Rectangular wound
- 6 Influence of the shape of the wound
- 7 Discussion, recommendations and conclusions

Next section

- 1 Biological background
- 2 Mathematical model
- 3 Analytical solutions
- 4 Numerical methods
- 5 Simulations
 - Circular wound
 - Rectangular wound
- 6 Influence of the shape of the wound
- 7 Discussion, recommendations and conclusions

Biological background

Heart attack



Biological background

Stem cell treatment

In order to avoid the formation of scar tissue on the wound:

- Stem cells are injected which secrete, among others, the growth factor $TG-\beta$, which enhances angiogenesis:
 - ▶ endothelial cells are provoked to move towards the wound (chemotaxis);
 - ▶ endothelial cells are provoked to divide.
- After the enhanced angiogenesis, vessels have been formed in the damaged part of the heart.

Biological background

Stem cell treatment

In order to avoid the formation of scar tissue on the wound:

- Stem cells are injected which secrete, among others, the growth factor $TG-\beta$, which enhances angiogenesis:
 - ▶ endothelial cells are provoked to move towards the wound (chemotaxis);
 - ▶ endothelial cells are provoked to divide.
- After the enhanced angiogenesis, vessels have been formed in the damaged part of the heart.

Biological background

Stem cell treatment

In order to avoid the formation of scar tissue on the wound:

- Stem cells are injected which secrete, among others, the growth factor $TG-\beta$, which enhances angiogenesis:
 - ▶ endothelial cells are provoked to move towards the wound (chemotaxis);
 - ▶ endothelial cells are provoked to divide.
- After the enhanced angiogenesis, vessels have been formed in the damaged part of the heart.

Biological background

Stem cell treatment

In order to avoid the formation of scar tissue on the wound:

- Stem cells are injected which secrete, among others, the growth factor $TG-\beta$, which enhances angiogenesis:
 - ▶ endothelial cells are provoked to move towards the wound (chemotaxis);
 - ▶ endothelial cells are provoked to divide.
- After the enhanced angiogenesis, vessels have been formed in the damaged part of the heart.

Question

How many stem cells should be injected when aiming at avoiding the formation of scar tissue?

Next section

- 1 Biological background
- 2 Mathematical model**
- 3 Analytical solutions
- 4 Numerical methods
- 5 Simulations
 - Circular wound
 - Rectangular wound
- 6 Influence of the shape of the wound
- 7 Discussion, recommendations and conclusions

Mathematical model

We observed two models:

- A model based on the work of Byrne et al;
- And a model based on the work of Maggelakis.

We choose to work with the *first* model since it is biologically the most extensive and mathematically the bigger challenge.

Mathematical model

We observed two models:

- A model based on the work of Byrne et al;
- And a model based on the work of Maggelakis.

We choose to work with the *first* model since it is biologically the most extensive and mathematically the bigger challenge.

Mathematical model

We observed two models:

- A model based on the work of Byrne et al;
- And a model based on the work of Maggelakis.

We choose to work with the *first* model since it is biologically the most extensive and mathematically the bigger challenge.

Variables

- $m(\mathbf{x}, t)$: number of stem cells;
- $c(\mathbf{x}, t)$: concentration TG- β ;
- $n(\mathbf{x}, t)$: capillary tip density;
- $\rho(\mathbf{x}, t)$: vessel density.

Mathematical model

Number of stem cells

$$\frac{\partial m}{\partial t} = -\beta_1 m,$$

- $$m(\mathbf{x}, 0) = \begin{cases} m_0, & \mathbf{x} \in \Omega_w, \\ 0, & \mathbf{x} \in \Omega \setminus \Omega_w. \end{cases}$$

Concentration TG- β (attractor)

$$\frac{\partial c}{\partial t} - \underbrace{D_1 \nabla \cdot (\nabla c)}_{\text{random walk}} + \lambda c = \alpha m,$$

Mathematical model

Number of stem cells

$$\frac{\partial m}{\partial t} = -\beta_1 m,$$

- $$m(\mathbf{x}, 0) = \begin{cases} m_0, & \mathbf{x} \in \Omega_w, \\ 0, & \mathbf{x} \in \Omega \setminus \Omega_w. \end{cases}$$

Concentration TG- β (attractor)

$$\frac{\partial c}{\partial t} - \underbrace{D_1 \nabla \cdot (\nabla c)}_{\text{random walk}} + \lambda c = \alpha m,$$

- $$c(\mathbf{x}, 0) = 0,$$

- $$\frac{\partial c}{\partial n} \Big|_{\Gamma} = 0.$$

Mathematical model

Number of stem cells

$$\frac{\partial m}{\partial t} = -\beta_1 m,$$

$$* m(\mathbf{x}, 0) = \begin{cases} m_0, & \mathbf{x} \in \Omega_w, \\ 0, & \mathbf{x} \in \Omega \setminus \Omega_w. \end{cases}$$

Concentration TG- β (attractor)

$$\frac{\partial c}{\partial t} - \underbrace{D_1 \nabla \cdot (\nabla c)}_{\text{random walk}} + \lambda c = \alpha m,$$

- $c(\mathbf{x}, 0) = 0,$
- $\frac{\partial c}{\partial \hat{n}} \Big|_{\Gamma} = 0.$

Mathematical model

Number of stem cells

$$\frac{\partial m}{\partial t} = -\beta_1 m,$$

Concentration TG- β (attractor)

$$\frac{\partial c}{\partial t} - \underbrace{D_1 \nabla \cdot (\nabla c)}_{\text{random walk}} + \lambda c = \alpha m,$$

- $c(\mathbf{x}, 0) = 0,$
- $\frac{\partial c}{\partial \hat{n}} \Big|_{\Gamma} = 0.$

Mathematical model

Capillary tip density

$$\frac{\partial n}{\partial t} + \underbrace{\chi_1 \nabla \cdot (n \nabla c)}_{\text{chemotaxis}} - D_2 \nabla \cdot (\nabla n) = \underbrace{\alpha_0 \rho c + \alpha_1 H(c - \hat{c}) n c - \beta_2 n \rho}_{\text{bifurcations and anastomosis}}$$

- $n(\mathbf{x}, 0) = 0,$
- $\chi_1 n \frac{\partial c}{\partial \hat{n}} - D_2 \frac{\partial n}{\partial \hat{n}} \Big|_{\Gamma} = 0.$

Vessel density

$$\frac{\partial \rho}{\partial t} - \epsilon \nabla \cdot (\nabla \rho) + \gamma(\rho - \rho_{eq}) = \underbrace{(\mu_1 \nabla n - \chi_2 n \nabla c)}_{\text{snail trail}} \cdot \frac{\mathbf{x}}{\|\mathbf{x}\|},$$

Mathematical model

Capillary tip density

$$\frac{\partial n}{\partial t} + \underbrace{\chi_1 \nabla \cdot (n \nabla c)}_{\text{chemotaxis}} - D_2 \nabla \cdot (\nabla n) = \underbrace{\alpha_0 \rho c + \alpha_1 H(c - \hat{c}) n c - \beta_2 n \rho}_{\text{bifurcations and anastomosis}}$$

- $n(\mathbf{x}, 0) = 0,$
- $\chi_1 n \frac{\partial c}{\partial \hat{n}} - D_2 \frac{\partial n}{\partial \hat{n}} \Big|_{\Gamma} = 0.$

Vessel density

$$\frac{\partial \rho}{\partial t} - \epsilon \nabla \cdot (\nabla \rho) + \gamma(\rho - \rho_{eq}) = \underbrace{(\mu_1 \nabla n - \chi_2 n \nabla c)}_{\text{snail trail}} \cdot \frac{\mathbf{x}}{\|\mathbf{x}\|},$$

$$\rho(\mathbf{x}, 0) = \begin{cases} 0, & \mathbf{x} \in \Omega_w, \\ \rho_{eq}, & \mathbf{x} \in \Omega \setminus \Omega_w, \end{cases}$$

$$\rho|_{\Gamma} = \rho_{eq}$$

Mathematical model

Capillary tip density

$$\frac{\partial n}{\partial t} + \underbrace{\chi_1 \nabla \cdot (n \nabla c)}_{\text{chemotaxis}} - D_2 \nabla \cdot (\nabla n) = \underbrace{\alpha_0 \rho c + \alpha_1 H(c - \hat{c}) n c - \beta_2 n \rho}_{\text{bifurcations and anastomosis}}$$

- $n(\mathbf{x}, 0) = 0,$
- $\chi_1 n \frac{\partial c}{\partial \mathbf{n}} - D_2 \frac{\partial n}{\partial \mathbf{n}} \Big|_{\Gamma} = 0.$

Vessel density

$$\frac{\partial \rho}{\partial t} - \epsilon \nabla \cdot (\nabla \rho) + \gamma(\rho - \rho_{eq}) = \underbrace{(\mu_1 \nabla n - \chi_2 n \nabla c)}_{\text{snail trail}} \cdot \frac{\mathbf{x}}{\|\mathbf{x}\|},$$

- $\rho(\mathbf{x}, 0) = \begin{cases} 0, & \mathbf{x} \in \Omega_w, \\ \rho_{eq}, & \mathbf{x} \in \Omega \setminus \Omega_w, \end{cases}$
- $\rho|_{\Gamma} = \rho_{eq}.$

Mathematical model

Capillary tip density

$$\frac{\partial n}{\partial t} + \underbrace{\chi_1 \nabla \cdot (n \nabla c)}_{\text{chemotaxis}} - D_2 \nabla \cdot (\nabla n) = \underbrace{\alpha_0 \rho c + \alpha_1 H(c - \hat{c}) n c - \beta_2 n \rho}_{\text{bifurcations and anastomosis}}$$

- $n(\mathbf{x}, 0) = 0,$
- $\chi_1 n \frac{\partial c}{\partial \mathbf{n}} - D_2 \frac{\partial n}{\partial \mathbf{n}} \Big|_{\Gamma} = 0.$

Vessel density

$$\frac{\partial \rho}{\partial t} - \epsilon \nabla \cdot (\nabla \rho) + \gamma(\rho - \rho_{eq}) = \underbrace{(\mu_1 \nabla n - \chi_2 n \nabla c)}_{\text{snail trail}} \cdot \frac{\mathbf{x}}{\|\mathbf{x}\|},$$

- $\rho(\mathbf{x}, 0) = \begin{cases} 0, & \mathbf{x} \in \Omega_w, \\ \rho_{eq}, & \mathbf{x} \in \Omega \setminus \Omega_w, \end{cases}$
- $\rho|_{\Gamma} = \rho_{eq}.$

Mathematical model

Question

Which numerical technique should be used?

Next section

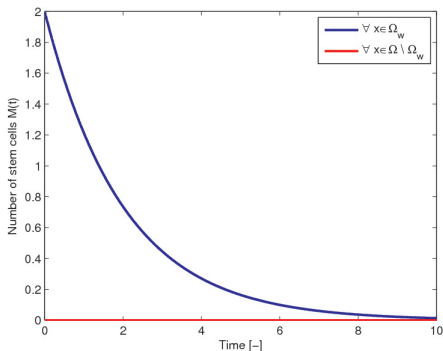
- 1 Biological background
- 2 Mathematical model
- 3 Analytical solutions**
- 4 Numerical methods
- 5 Simulations
 - Circular wound
 - Rectangular wound
- 6 Influence of the shape of the wound
- 7 Discussion, recommendations and conclusions

Analytical solutions

Number of stem cells

The number of stem cells decreases exponentially:

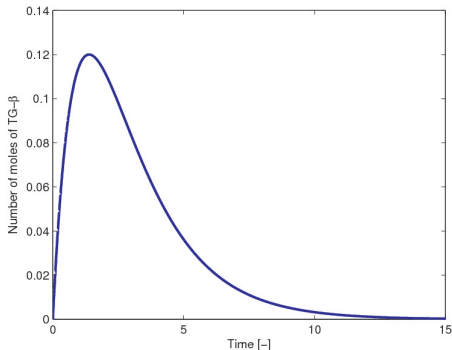
$$m(\mathbf{x}, t) = \begin{cases} m_0 e^{-\beta_1 t} & \mathbf{x} \in \Omega_w, \\ 0 & \mathbf{x} \in \Omega \setminus \Omega_w. \end{cases}$$



Analytical solutions

Number of TG- β

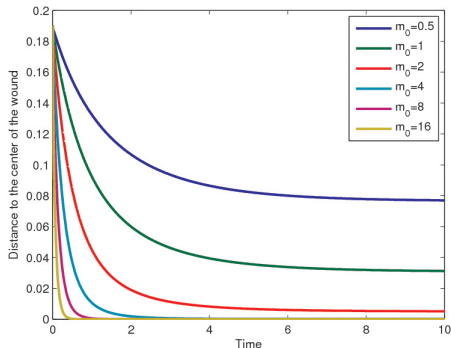
The number of TG- β is determined by $\bar{c}(t) = \int_{\Omega} c(\mathbf{x}, t) d\Omega$.



Analytical solutions

Characteristics of the capillary tip density

The only parameter not fixed by biology, is the number of injected stem cells m_0 .



Speed of the characteristics:

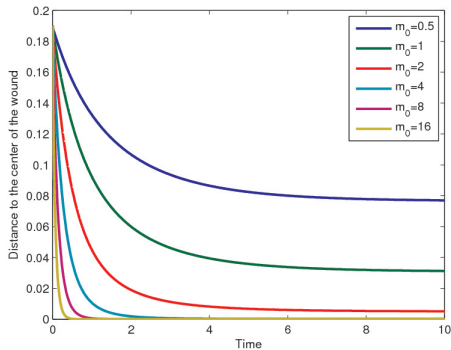
$$\frac{dx}{dt} = \chi_1 \frac{\partial c}{\partial x}.$$

Boundary wound: $\delta = 0.2$.

Analytical solutions

Characteristics of the capillary tip density

The only parameter not fixed by biology, is the number of injected stem cells m_0 .



Speed of the characteristics:
$$\frac{dx}{dt} = \chi_1 \frac{\partial c}{\partial x}.$$

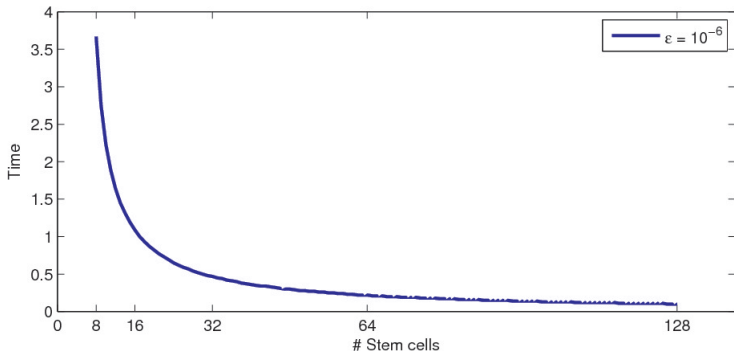
Boundary wound: $\delta = 0.2$.

Number of stem cells is not always enough for the characteristics to converge to the center of the wound!

Analytical solutions

Characteristics of the capillary tip density

The wound will have sufficient blood supply if there exists a time \tilde{t} such that, $\tilde{t} = \operatorname{argmin}_{t \in (0, T]} \{t \in (0, T] : |x(t)| < \epsilon\}$.



Next section

- 1 Biological background
- 2 Mathematical model
- 3 Analytical solutions
- 4 Numerical methods**
- 5 Simulations
 - Circular wound
 - Rectangular wound
- 6 Influence of the shape of the wound
- 7 Discussion, recommendations and conclusions

Numerical methods

Mesh Péclet number

mesh Péclet number

$$Pe_m = \frac{v\Delta x}{D},$$

where v is the absolute speed and D the diffusion coefficient.

If Pe_m is relatively large, the problem is dominated by convection and the hyperbolicity of the problem increases.

The equation for the capillary tip density was

$$\frac{\partial n}{\partial t} + \chi_1 \nabla \cdot (n \nabla c) - D_2 \nabla \cdot (\nabla n) = \alpha_0 \rho c + \alpha_1 H(c - \hat{c}) n c - \beta_2 n \rho,$$

hence $Pe_m = \frac{|\chi_1 \nabla c| \Delta x}{D_2}$.

Numerical methods

Mesh Péclet number

mesh Péclet number

$$Pe_m = \frac{v\Delta x}{D},$$

where v is the absolute speed and D the diffusion coefficient.

If Pe_m is relatively large, the problem is dominated by convection and the hyperbolicity of the problem increases.

The equation for the capillary tip density was

$$\frac{\partial n}{\partial t} + \chi_1 \nabla \cdot (n \nabla c) - D_2 \nabla \cdot (\nabla n) = \alpha_0 \rho c + \alpha_1 H(c - \hat{c}) n c - \beta_2 n \rho,$$

$$\text{hence } Pe_m = \frac{|\chi_1 \nabla c| \Delta x}{D_2}.$$

Numerical methods

Mesh Péclet number

mesh Péclet number

$$Pe_m = \frac{v\Delta x}{D},$$

where v is the absolute speed and D the diffusion coefficient.

If Pe_m is relatively large, the problem is dominated by convection and the hyperbolicity of the problem increases.

The equation for the capillary tip density was

$$\frac{\partial n}{\partial t} + \chi_1 \nabla \cdot (n \nabla c) - D_2 \nabla \cdot (\nabla n) = \alpha_0 \rho c + \alpha_1 H(c - \hat{c}) n c - \beta_2 n \rho,$$

$$\text{hence } Pe_m = \frac{|\chi_1 \nabla c| \Delta x}{D_2}.$$

Numerical methods

- We successfully implemented the finite element method for simulating the model with certain parameters;
- The chemotaxis term was suspected to have more influence than we used for these simulations;
- Therefore, we increased the chemotaxis coefficient χ_1 , which increased the mesh Péclet number $Pe_m = \frac{|\chi_1 \nabla c| \Delta x}{D_2}$;
- The mesh Péclet number became too high, the hyperbolicity of the problem increased and the finite element method was not sufficient anymore;
- A different numerical method was needed.

The discontinuous Galerkin method

Numerical methods

- We successfully implemented the finite element method for simulating the model with certain parameters;
- The chemotaxis term was suspected to have more influence than we used for these simulations;
- Therefore, we increased the chemotaxis coefficient χ_1 , which increased the mesh Péclet number $Pe_m = \frac{|\chi_1 \nabla c| \Delta x}{D_2}$;
- The mesh Péclet number became too high, the hyperbolicity of the problem increased and the finite element method was not sufficient anymore;
- A different numerical method was needed.

The discontinuous Galerkin method

Numerical methods

- We successfully implemented the finite element method for simulating the model with certain parameters;
- The chemotaxis term was suspected to have more influence than we used for these simulations;
- Therefore, we increased the chemotaxis coefficient χ_1 , which increased the mesh Péclet number $Pe_m = \frac{|\chi_1 \nabla c| \Delta x}{D_2}$;
- The mesh Péclet number became too high, the hyperbolicity of the problem increased and the finite element method was not sufficient anymore;
- A different numerical method was needed.

The discontinuous Galerkin method

Numerical methods

- We successfully implemented the finite element method for simulating the model with certain parameters;
- The chemotaxis term was suspected to have more influence than we used for these simulations;
- Therefore, we increased the chemotaxis coefficient χ_1 , which increased the mesh Péclet number $Pe_m = \frac{|\chi_1 \nabla c| \Delta x}{D_2}$;
- The mesh Péclet number became too high, the hyperbolicity of the problem increased and the finite element method was not sufficient anymore;
- A different numerical method was needed.

The discontinuous Galerkin method

Numerical methods

- We successfully implemented the finite element method for simulating the model with certain parameters;
- The chemotaxis term was suspected to have more influence than we used for these simulations;
- Therefore, we increased the chemotaxis coefficient χ_1 , which increased the mesh Péclet number $Pe_m = \frac{|\chi_1 \nabla c| \Delta x}{D_2}$;
- The mesh Péclet number became too high, the hyperbolicity of the problem increased and the finite element method was not sufficient anymore;
- A different numerical method was needed.

The discontinuous Galerkin method

Numerical methods

- We successfully implemented the finite element method for simulating the model with certain parameters;
- The chemotaxis term was suspected to have more influence than we used for these simulations;
- Therefore, we increased the chemotaxis coefficient χ_1 , which increased the mesh Péclet number $Pe_m = \frac{|\chi_1 \nabla c| \Delta x}{D_2}$;
- The mesh Péclet number became too high, the hyperbolicity of the problem increased and the finite element method was not sufficient anymore;
- A different numerical method was needed.

The discontinuous Galerkin method

Numerical methods

DG vs FEM

	DG	FEM
complicated geometries	yes	yes
global solution	discontinuous	continuous
smoothness	local	global
jumps possible	yes	no

Numerical methods

DG vs FEM

	DG	FEM
complicated geometries	yes	yes
global solution	discontinuous	continuous
smoothness	local	global
jumps possible	yes	no

Numerical methods

DG vs FEM

	DG	FEM
complicated geometries	yes	yes
global solution	discontinuous	continuous
smoothness	local	global
jumps possible	yes	no

Numerical methods

The discontinuous Galerkin method

For a one-dimensional problem:

- Partition the domain into N elements;
- Each element is denoted by $e_j = [x_{j-1/2}, x_{j+1/2}]$, for $1 \leq j \leq N$, with element size Δx ;
- The solution in element e_j is approximated by

$$u_h(x, t) = \sum_{l=0}^K \hat{u}_j^l(t) \varphi_j^l(x),$$

which is a linear combination of polynomials of order $l = 0$ up to $l = K$;

- High accuracy can be obtained.

Numerical methods

The discontinuous Galerkin method

For a one-dimensional problem:

- Partition the domain into N elements;
- Each element is denoted by $e_j = [x_{j-1/2}, x_{j+1/2}]$, for $1 \leq j \leq N$, with element size Δx ;
- The solution in element e_j is approximated by

$$u_h(x, t) = \sum_{l=0}^K \hat{u}_j^l(t) \varphi_j^l(x),$$

which is a linear combination of polynomials of order $l = 0$ up to $l = K$;

- High accuracy can be obtained.

Numerical methods

The discontinuous Galerkin method

For a one-dimensional problem:

- Partition the domain into N elements;
- Each element is denoted by $e_j = [x_{j-1/2}, x_{j+1/2}]$, for $1 \leq j \leq N$, with element size Δx ;
- The solution in element e_j is approximated by

$$u_h(x, t) = \sum_{l=0}^K \hat{u}_j^l(t) \varphi_j^l(x),$$

which is a linear combination of polynomials of order $l = 0$ up to $l = K$;

- High accuracy can be obtained.

Numerical methods

The discontinuous Galerkin method

- In order to do this we scale each element

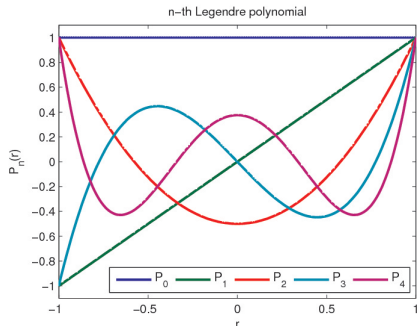
$e_j = [x_{j-1/2}, x_{j+1/2}]$ to the reference element $[-1, 1]$;

- For the polynomials we use the Legendre polynomials which are defined on the local element $[-1, 1]$.

Numerical methods

The discontinuous Galerkin method

- In order to do this we scale each element $e_j = [x_{j-1/2}, x_{j+1/2}]$ to the reference element $[-1, 1]$;
- For the polynomials we use the Legendre polynomials which are defined on the local element $[-1, 1]$.



Numerical methods

The discontinuous Galerkin method

We need to determine the coefficients corresponding to the polynomials for all elements and for all time steps in order to determine the solution

$$u_h(x, t) = \sum_{l=0}^K \hat{u}_j^l(t) \varphi_j^l(x),$$

which is, after scaling the element,

$$u_h(x, t) = \sum_{l=0}^K \hat{u}_j^l(t) P_l(r).$$

Numerical methods

The discontinuous Galerkin method

The coefficients $\hat{u}_j^l(t)$ are determined by deriving the weak formulation and numerically solving equations of matrix-vector products.

For a higher dimensional model the discontinuous Galerkin method works in a similar way.

Limiting

If there is no diffusion and a discontinuity stays a discontinuity, as in the advection equation, a limiter should be used in order to prevent wiggles.

Numerical methods

The discontinuous Galerkin method

The coefficients $\hat{u}_j^l(t)$ are determined by deriving the weak formulation and numerically solving equations of matrix-vector products.

For a higher dimensional model the discontinuous Galerkin method works in a similar way.

Limiting

If there is no diffusion and a discontinuity stays a discontinuity, as in the advection equation, a limiter should be used in order to prevent wiggles.

Numerical methods

The discontinuous Galerkin method

The coefficients $\hat{u}_j^l(t)$ are determined by deriving the weak formulation and numerically solving equations of matrix-vector products.

For a higher dimensional model the discontinuous Galerkin method works in a similar way.

Limiting

If there is no diffusion and a discontinuity stays a discontinuity, as in the advection equation, a limiter should be used in order to prevent wiggles.

Next section

- 1 Biological background
- 2 Mathematical model
- 3 Analytical solutions
- 4 Numerical methods
- 5 Simulations**
 - Circular wound
 - Rectangular wound
- 6 Influence of the shape of the wound
- 7 Discussion, recommendations and conclusions

Next subsection

- 1 Biological background
- 2 Mathematical model
- 3 Analytical solutions
- 4 Numerical methods
- 5 Simulations**
 - Circular wound
 - Rectangular wound
- 6 Influence of the shape of the wound
- 7 Discussion, recommendations and conclusions

Simulations

DG - circular wound

Two-dimensional model rewritten into polar coordinates.

The concentration $TG-\beta$, $c(r, t)$:

Simulations

DG - circular wound

The capillary tip density, $n(r, t)$:

Simulations

DG - circular wound

The vessel density, $\rho(r, t)$, with discontinuous initial condition:

Simulations

DG - circular wound

The vessel density, $\rho(r, t)$:

Next subsection

- 1 Biological background
- 2 Mathematical model
- 3 Analytical solutions
- 4 Numerical methods
- 5 Simulations**
 - Circular wound
 - **Rectangular wound**
- 6 Influence of the shape of the wound
- 7 Discussion, recommendations and conclusions

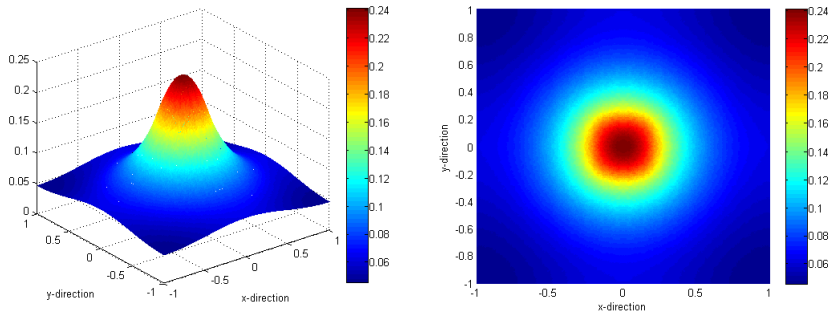
Simulations

DG - rectangular wound

Simulations for a rectangular wound, using:

- rectangular elements e_{ij} ,
- relatively low order of polynomials.

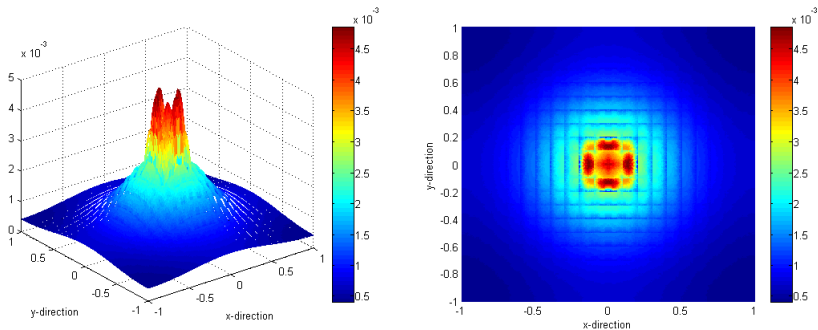
The concentration $TG-\beta$, $c(\mathbf{x}, t)$, at $t = 0.5$:



Simulations

DG - rectangular wound

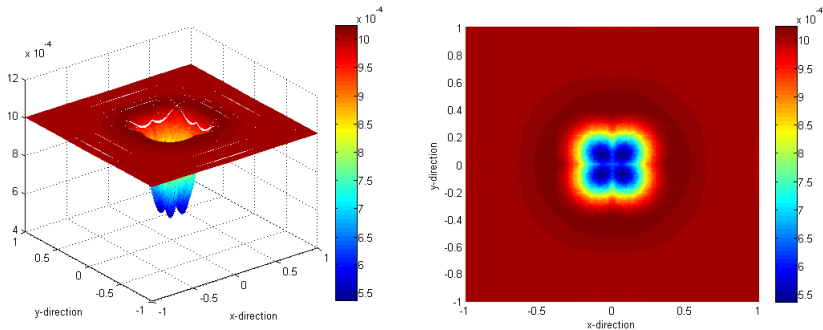
The capillary tip density, $n(\mathbf{x}, t)$, at $t = 0.5$:



Simulations

DG - rectangular wound

The vessel density, $\rho(\mathbf{x}, t)$, at $t = 0.5$:



Next section

- 1 Biological background
- 2 Mathematical model
- 3 Analytical solutions
- 4 Numerical methods
- 5 Simulations
 - Circular wound
 - Rectangular wound
- 6 Influence of the shape of the wound**
- 7 Discussion, recommendations and conclusions

Influence of the shape of the wound

The shapes

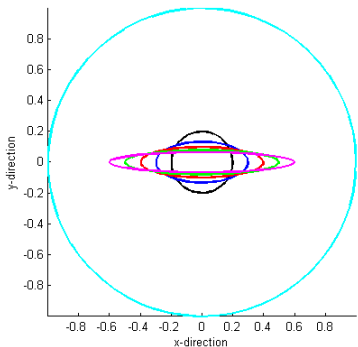
Question

What is the influence of the shape of the wound?

Compare simulations with:

- Wounds of different shapes;
- Wounds with the same area;
- The same parameter values.

We used the finite element method.



Influence of the shape of the wound

The shapes

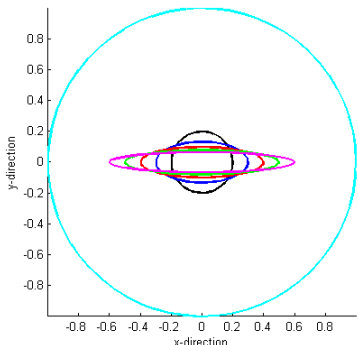
Question

What is the influence of the shape of the wound?

Compare simulations with:

- Wounds of different shapes;
- Wounds with the same area;
- The same parameter values.

We used the finite element method.



Influence of the shape of the wound

The shapes

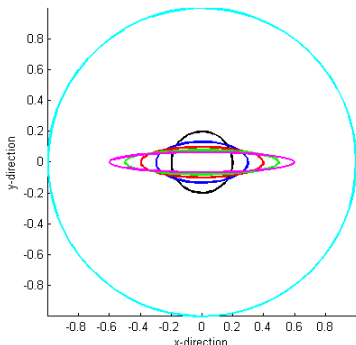
Question

What is the influence of the shape of the wound?

Compare simulations with:

- Wounds of different shapes;
- Wounds with the same area;
- The same parameter values.

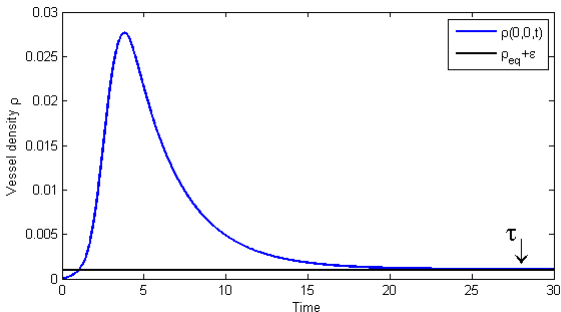
We used the finite element method.



Influence of the shape of the wound

Vessel density in the center of the wound

We monitor the center of the wound $(0,0)$ and determine the time τ , where the vessel density drops below $\rho_{eq} + \epsilon$, with a small ϵ .



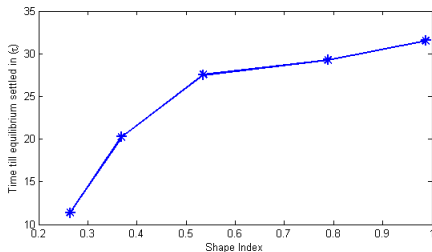
Influence of the shape of the wound

Shape Index

Shape Index (SI):

$$SI(\Omega) = \frac{4\pi A(\Omega)}{l^2(\Omega)},$$

where $SI(\Omega) = 1$ corresponds to a circle.



Wound with
 $SI(\Omega) = \pm 0.33$ healed
two times faster than a
wound with $SI(\Omega) = 1$.

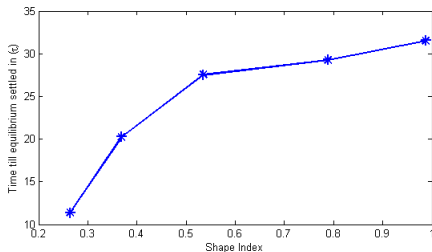
Influence of the shape of the wound

Shape Index

Shape Index (SI):

$$SI(\Omega) = \frac{4\pi A(\Omega)}{l^2(\Omega)},$$

where $SI(\Omega) = 1$ corresponds to a circle.



Wound with $SI(\Omega) = \pm 0.33$ healed *two times faster* than a wound with $SI(\Omega) = 1$.

Next section

- 1 Biological background
- 2 Mathematical model
- 3 Analytical solutions
- 4 Numerical methods
- 5 Simulations
 - Circular wound
 - Rectangular wound
- 6 Influence of the shape of the wound
- 7 Discussion, recommendations and conclusions

Discussion, recommendations and conclusions

Part 1/4

We developed a model for angiogenesis under the injection of stem cells onto the damaged part of the heart after an infarction.

- Are the initial conditions a reflection of reality?
- Investigate realistic values for the parameters.
- What is the influence of multiple injections of stem cells instead of a single injection?
- The model is only applicable for a single wound.

Discussion, recommendations and conclusions

Part 1/4

We developed a model for angiogenesis under the injection of stem cells onto the damaged part of the heart after an infarction.

- Are the initial conditions a reflection of reality?
- Investigate realistic values for the parameters.
- What is the influence of multiple injections of stem cells instead of a single injection?
- The model is only applicable for a single wound.

Discussion, recommendations and conclusions

Part 1/4

We developed a model for angiogenesis under the injection of stem cells onto the damaged part of the heart after an infarction.

- Are the initial conditions a reflection of reality?
- Investigate realistic values for the parameters.
- What is the influence of multiple injections of stem cells instead of a single injection?
- The model is only applicable for a single wound.

Discussion, recommendations and conclusions

Part 1/4

We developed a model for angiogenesis under the injection of stem cells onto the damaged part of the heart after an infarction.

- Are the initial conditions a reflection of reality?
- Investigate realistic values for the parameters.
- What is the influence of multiple injections of stem cells instead of a single injection?
- The model is only applicable for a single wound.

Discussion, recommendations and conclusions

Part 1/4

We developed a model for angiogenesis under the injection of stem cells onto the damaged part of the heart after an infarction.

- Are the initial conditions a reflection of reality?
- Investigate realistic values for the parameters.
- What is the influence of multiple injections of stem cells instead of a single injection?
- The model is only applicable for a single wound.

Discussion, recommendations and conclusions

Part 2/4

Using the method of characteristics, we are able to quickly estimate the efficiency of treatment with respect to the number of stem cells injected.

- In our simulations we need at least $m_0 = 8$ (million) stem cells.

Discussion, recommendations and conclusions

Part 2/4

Using the method of characteristics, we are able to quickly estimate the efficiency of treatment with respect to the number of stem cells injected.

- In our simulations we need at least $m_0 = 8$ (million) stem cells.

Discussion, recommendations and conclusions

Part 3/4

We successfully implemented the finite element (FEM) and the discontinuous Galerkin (DG) method for the one and two-dimensional problem.

- With FEM we found that the shape of the wound influences the healing time: a flatter wound is healed faster;
- Unfortunately, FEM was not sufficient anymore when we increased the hyperbolicity of the model;

Discussion, recommendations and conclusions

Part 3/4

We successfully implemented the finite element (FEM) and the discontinuous Galerkin (DG) method for the one and two-dimensional problem.

- With FEM we found that the shape of the wound influences the healing time: a flatter wound is healed faster;
- Unfortunately, FEM was not sufficient anymore when we increased the hyperbolicity of the model;

Discussion, recommendations and conclusions

Part 3/4

We successfully implemented the finite element (FEM) and the discontinuous Galerkin (DG) method for the one and two-dimensional problem.

- With FEM we found that the shape of the wound influences the healing time: a flatter wound is healed faster;
- Unfortunately, FEM was not sufficient anymore when we increased the hyperbolicity of the model;

Discussion, recommendations and conclusions

Part 4/4

- DG is very accurate and can handle hyperbolic problems, however the method, in particular in more dimensions, suffers from large computation time, which makes the method unattractive for now;
- Note that we only implemented DG for circular and rectangular wounds.

Discussion, recommendations and conclusions

Part 4/4

- DG is very accurate and can handle hyperbolic problems, however the method, in particular in more dimensions, suffers from large computation time, which makes the method unattractive for now;
- Note that we only implemented DG for circular and rectangular wounds.

Thank you for your attention!
Questions?